Finding Non Dominant Electrodes Placed in Electroencephalography (EEG) for Eye State Classification using Rule Mining

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Abstract-Electroencephalography is a measure of brain activity by wave analysis; it consist number of electrodes. Finding most non-dominant electrode positions in Eye state classification is important task for classification. The proposed work is identifying which electrodes are less responsible for classification. This is a feature selection step required for optimal EEG channel selection. Feature selection is a mechanism for subset selection of input features, in this work input features are EEG Electrodes. Most Non Dominant (MND), gives irrelevant input electrodes in eye state classification and thus it, reduces computation cost. MND set creation completed using different stages. Stages includes, first extreme value removal from electroencephalogram (EEG) corpus for data cleaning purpose. Then next step is attribute selection, this is a preprocessing step because it is completed before classification step. MND set gives electrodes they are less responsible for classification and if any EEG electrode corpus wants to remove feature present in this set, then time and space required to build the classification model is (20%) less than as compare to all electrodes for the same, and accuracy of classification not very much affected. The proposed article uses different attribute evaluation algorithm with Ranker Search Method.

Keywords—Electroencephalography (EEG); Most Non Dominant (MND); Ranker algorithm; classification; EEG

I. INTRODUCTION

The MND feature subset selection is a part of corpus preprocessing, and it is useful for classification model building as a supervised learning .Classification is one of the task performed by data mining tools and applicable in different area of biomedical electrical devices such as EEG. ECG(Electrocardiograms), EMG(Electromyography), EOG(Electrooculography), Actigraph devices etc. These devices are popular devices for recognizing of different types of disease like Sleep Apnea diagnosis[1] using ECG, driving drowsing using EEG[2],EEG and electromyography (EMG) enable communication for people with severe disabilities [20], muscles activity using EOG[3], and military operation using EEG[21] etc. These are the motivational points for proposed work because the article finds those positions electrode they are less responsible for classification then the removal of those electrodes minimize the size of devices. The present work is performed with EEG electrode data having 16 electrodes and 14892 instances [4,5]. This uses the instance based classifier (K*), because based on statistic of data and nature of data spread over the corpus found it is best among

other classifier the result of this present in literature [6, 7], [28], [33], [38]. Method selects either one electrode, two electrode or three electrodes based on how much search space the corpus wants to reduce. Its outcome generated from different attribute selection search with attribute evaluation techniques [8], [37]. Here it is 11 different combination of search with evaluation techniques. Then generating rules using Apriori algorithm [9], it gives frequent electrodes which are placed in ranked as a last four sequences, it also depends how many last feature ranked matrix the corpus wants to create. Here it is 11*4, where 11 are a Row value and 4 is a column value. Ranker Search with different attribute evaluation algorithms shown in Figure [1].Rankers Algorithm is an algorithm useful for ranking of attributes by their individual evaluation [10]. Here three attribute evaluation methods are defined.

1) **Info Gain Attribute evaluation**: Evaluate the worth of an attribute by measuring the gain ratio with respect to the class.

2) **Classifier Attribute Evaluation**: Evaluate the work of n attribute by using a user specified classifier.

3) **OneR Attribute Evaluation**: Evaluate the work of an attribute by using the oneR classifier.

II. ASSOCIATION RULE MINING

Association Rule Mining is used here for obtaining frequent set they are correlated with each other using support and confidence parameters [11-13].

Support is define as how frequently a specific item set occur in the data base (the percentage of transactions that contain all of the items in the item set, here the set of items are electrodes present in corpus and the transaction is the different method used for evaluation).

Confidence is the probability that items in RHS (Right Hand Side) will occur given that the items in LHS (left hand side) occurs. It Computed as

Confidence (LHS) =>Support (LHS U RHS)/ Support (LHS) Electrode1 => Electrode2 [0.588, 0.88]

If Electrode1 is selected in MND set, then Electrode2 also selected in MND set if it will satisfies minimum support and minimum confidence value. Left hand side electrode as Antecedent and Right hand side electrode [RHS] as consequent frequency.

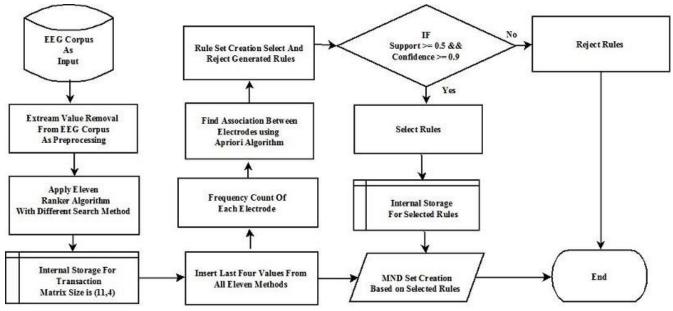


Fig. 1. Flowchart of Proposed Work

III. ELECTROENCEPHALOGRAPHY (EEG)

EEG is useful for measuring brain activity. During the test very little electricity is passed between the electrodes and skin. EEG usually takes 30-60 minutes. The technician will put a sticky gel adhesive on 16 to 25 electrodes at various spots on our scalp [14]. There are various spatial resolution of EEG systems like 10/20, 10/10, 10/5 systems as relative had surface based positioning system. The international 10/20 system a standard system for electrode positioning with 21 electrodes extended to higher density electrode such as 10/10 and 10/5 systems allowing more than 300 electrode positions [15].

Here the proposed methodology is used in 10/20 system with 16 electrodes (AF3, F7, F3, AF3, F7, F3, FC5, T7, P7, O1, O2, P8, T8, FC6, F4, F8, and AF4).

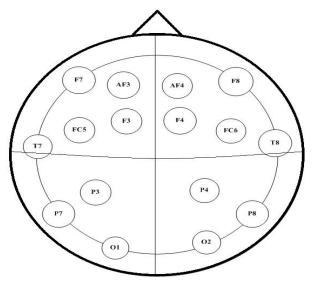


Fig. 2. EEG positioned electrodes 10/20

 TABLE I.
 Search Method used with Different Attribute

 Evaluators
 Evaluators

SEARCH METHOD + ATTRIBUTE EVALUATOR	TRANSACTION			
Ranker + InfoGainAttributeEval	T1			
Ranker + ChiSquaredAttributeEval	T2			
Ranker + ClassifierAttributeEval	T3			
Ranker + CorrelationAttributeEval	T4			
Ranker + CVAttributeEval	T5			
Ranker + FilteredAttributeEval	T6			
Ranker + GainRatioAttributeEval	T7			
Ranker + OneRAttributeEval	T8			
Ranker + ReliefFAttributeEval	T9			
Ranker + SignificanceAttributeEval	T10			
Ranker+SymmetricalUncertAttributeEval	T11			

IV. EEG CORPUS

The Corpus consists of 14980 instances with 15 features each (14 features representing the values of Electrodes and one as eye state (Boolean Variable)).Statistical Evaluation finds extreme values present in the corpus, here thirty eight instances (186, 899, 10387, 10674, 10675, 10676, 10677, 10678, 10679, 10680, 10681, 10682, 10683, 10684, 10685, 10686, 10687, 10688, 10689, 10690, 10691, 10692, 10693, 10694, 10695, 10696, 10697, 10698, 10699, 10700, 10701, 10702, 10704, 10707, 10708, 10709, 11510 and 13180) declared as extreme values in this, removal of it makes new corpus and it is having 14942 instances . The stored corpus as ordered to able to analyze temporal dependency 8220(55.01%) instances of the corpus corresponds to the eye open and 6722(44.99%) instances to the eye closed. EEG eye state dataset was donated by Rosler and Suendermann from Baden-Wuerttemberg Cooperative State University (DHBW), Stuttgart, Germany [4]. The output of the corpus "1" indicates

the eye-closed and "0" indicates the eye-open state.

V. EXTREME VALUE REMOVAL

The extreme value removal is a part of data cleaning step for data mining. The procedure for applying the extreme value theorem is to first establish that the function is continuous on the closed interval [16]. The next step is to determine the critical points in the given interval and evaluate the function at these critical points and at the end points of the interval. If the function f(x) is continuous on closed interval [a, b] then f(x)has both a maximum and a minimum on [a, b] [17]. In proposed method inter-quartile range [IQR] is used for extreme value calculations. IQR is major of variability based on dividing the dataset into quartiles [18].

VI. FEATURE SUBSET SELECTION

Feature Subset Selection is a task of data mining tool[25,26], it selects optimal feature subset for classifying the dataset but the literature shows the subset of optimal feature may or may not be optimal[19],[22-24]. The proposed work is searching Most Non Dominant features (MND) from the feature set. This performed by ranker algorithm and with different search methods. The outcome of this step is ranks of electrodes placed in scalp. Proposed work used different 11 algorithms for obtaining the ranks of electrodes (most to least dominant).

 TABLE II.
 TRANSACTION IN MATRICES WITH FOUR LAST DOMINANT ATTRIBUTES

Transaction	L4	L3	L2	L1
T1	O2	F7	FC5	F3
T2	O2	F7	FC5	F3
Т3	FC6	O2	FC5	F7
T4	P7	O1	FC5	T7
T5	F7	AF4	F8	AF3
T6	O2	F7	FC5	F3
T7	F7	FC5	O2	F3
T8	FC6	O2	FC5	F7
Т9	F3	F4	O2	P8
T10	P8	O2	F3	F7
T11	F7	FC5	O2	F3

VII. CLASSIFICATION

Classification is the task of data mining and it is a supervised learning. To classify EEG signals, various classification techniques present in literature [34-38]. The instances present in corpus for eye state recognition using EEG, these instances are classified in to two different classes, zero is for eye opened state and one is for eye closed state. The instance based classifier is a type of lazy classifier [27], and proposed method uses K* is a type of instance base classifier, after extreme value removal and attribute selection. The literature shows there are various statistical measures are used for analysis of classification outcomes generated from classification process [29-32].

VIII. PROPOSED METHODOLOGY FOR MND SET

The proposed methodology is use full for finding nondominant feature from feature set. If "n" number of features are used for classification of eye state recognition then the space and time requirement is very high but if using less no of features obtained from proposed method then this will save time and space requirement. MND set electrodes are always a most non-dominant electrodes they are less responsible for classification accuracy. The flowchart shows in figure [1], and described steps shows, how to get MND from feature subset results generated from previous step.

5.No.	LHS		RHS	Lift			
1	{}	=>	{F7}	} 0.8182 0.8181818		1	
2	{FC6}	=>	{FC5}	0.1818	1	1.375	
3	{FC6}	=>	{02}	0.1818	1	1.375	
4	{FC6}	=>	{F7}	0.1818	1	1.222222	
5	{P8}	=>	{F3}	0.1818	1	1.571429	
6	{P8}	=>	{02}	0.1818	1	1.375	
7	{F3}	=>	{02}	0.5455	0.8571429	1.178571	
8	{F3}	=>	{F7}	0.5455	0.8571429	1.047619	
9	{FC5}	=>	{F7}	0.6364	0.875	1.069444	
10	{02}	=>	{F7}	0.6364	0.875	1.069444	
11	{FC5, FC6}	=>	{02}	0.1818	1	1.375	
12	{FC6, O2}	=>	{FC5}	0.1818	1	1.375	
13	{FC5, FC6}	=>	{F7}	0.1818	1	1.222222	
14	{F7, FC6}	=>	{FC5}	0.1818	1	1.375	
15	{FC6, O2}	=>	{F7}	0.1818	1	1.222222	
16	{F7, FC6}	=>	{02}	0.1818	1	1.375	
17	{F3, P8}	=>	{02}	0.1818	1	1.375	
18	{O2, P8}	=>	{F3}	0.1818	1	1.571429	
19	{F3, FC5}	=>	{02}	0.3636	0.8	1.1	
20	{F3, FC5}	=>	{F7}	0.4545	1	1.222222	
21	{F3, F7}	=>	{FC5}	0.4545	0.8333333	1.145833	
22	{F3, O2}	=>	{F7}	0.4545	0.8333333	1.018519	
23	{F3, F7}	=>	{02}	0.4545	0.8333333	1.145833	
24	{FC5, O2}	=>	{F7}	0.5455	1	1.222222	
25	{F7, FC5}	=>	{02}	0.5455	0.8571429	1.178571	
26	{F7, O2}	=>	{FC5}	0.5455	0.8571429	1.178571	
27	{FC5, FC6, O2}	=>	{F7}	0.1818	1	1.222222	
28	{F7, FC5, FC6}	=>	{02}	0.1818	1	1.375	
29	{F7, FC6, O2}	=>	{FC5}	0.1818	1	1.375	
30	{F3, FC5, O2}	=>	{F7}	0.3636	1	1.222222	
31	{F3, F7, FC5}	=>	{02}	0.3636	0.8	1.1	
32	{F3, F7, O2}	=>	{FC5}	0.3636	0.8	1.1	

Fig. 3. Rule Generated from Apriori Algorithm

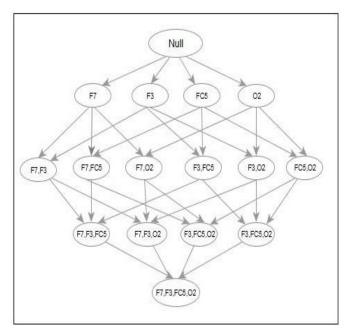


Fig. 4. Lattice occurs by Association Rule Mining

Algorithm 1: Most Non Dominant (MND) Feature Set Generation Algorithm

Input: D, I , T , C, MSupport.

- //D = Set of Electrodes.
- // I = Total Instances
- //T = Transactions
- //C = Corpus
- // L= Class label $\{0, 1\}$

//MSupport=Minimum Support

Output: MND set

Segment(C); // call this for creating a training, testing and validation set creation.

For i=1 To 11 do

For j=1 To 4 do

T[R] [C] = LRS(C);

// Call function for last 4 values from different feature ranker search with evaluation techniques

//Transaction Matrix insertion for Item Set (Electrode) placed last 4 positions.

MND=Apriori(T,Msupport); //Calling Apriori for frequent set generation for

End

Function Definition for Segment Creation from Corpus

R= R-Te; V= R; //Validation Set Creation Return (T, Te, V)

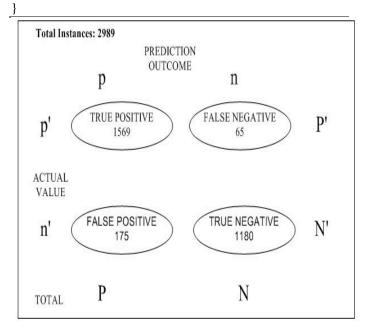


Fig. 5. Confusion Matrix on Removal of F7, FC5, O2

Function Definition for Last Ranked Set (LRS)

LRS(C)

For i=1 To 11 do For j=1 To 4 do

Ran[j] =Ranker (i); //Last 4 ranked value search and stored in array End //for End

Return (Ran[j]);

End }

Function Apriori Algorithm for Frequent Set Mining

Apriori (T, mSupport)

//*T* is the database and mSupport is the minimum support $F_1 = \{$ frequent items $\};$

For $(k=2; F_{k-1}! = \emptyset; k++)$

Ck= candidates generated from F_{k-1} //Cartesian product $F_{k-1} \times F_{k-1}$ and eliminating any k-1 size item set that is not frequent For each transaction do { //increment the count of all candidates in Fk that are contained in T

 F_k = candidates in C_k with minimum Support}

} end for inner for Return $\bigcup_k L_k$; }

IX. RESULT AND ANALYSIS

This study used Ranker Search with Attribute Evaluation technique for MND set creation shown in table[1], then for rule generated using association rule mining this task performed by using Apriori algorithm ,all the generated rules are shown in figure[3], and the lattice shown in figure [4], shows how many frequent set to be considered for rule generation, the rules which is having minimum support and confidence is highlighted in figure[3], this gives frequent items (Electrode) set ,here it is {FC5,O2,F7}. This set declared as MND set, removing of this electrodes from EEG corpus sufficiently decrease the space and time requirement to built the classification model. The accuracy towards the classification changed very less and this analysis outcome shown in table [3], figure[6]. The Confusion matrix shown in figure [5] and ROC curve shown in figure [7], evaluate the classifier performance here the classifier is Instance based classifier (K*), the classification accuracy is computed and it is mapped in table [3].

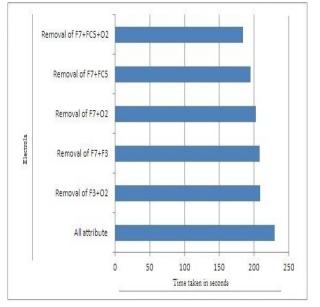


Fig. 6. Time duration with Removal of Different Attributes

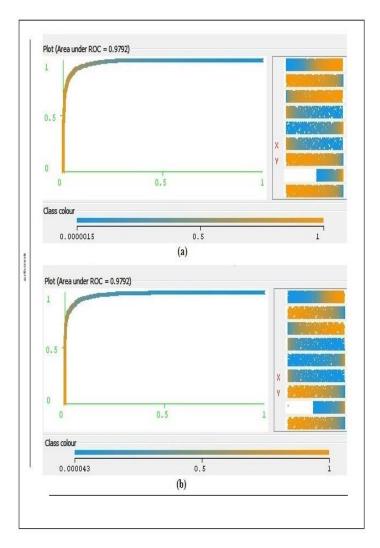


Fig. 7. ROC Curve removal on removal of F7, FC5, O2 (a) Threshold Value as 0 (b) Threshold value as 1 $\,$

X. CONCLUSION

This is the first study to investigate the characteristics of Most Non Dominant feature from feature space they are less responsible to build the classification model, the MND set always gives concept which feature removal sufficiently reduce space and time requirement to build the classification model. This result is tested with EEG corpus to investigate eye state, either it is closed or open. Approximate 20% of time is saved by removal of these three most dominant features as compare to all attributes considered for classification.

TABLE III. RES	ULT ANALYSIS AFTER REMOVAL OF ATTRIBUTES FROM FEATURE SET FROM EEG DATA SET
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Electrode Removal	TP Rate	FP Rate	Precision	Recall	F-Measure	MCC	ROC	PRC	Accuracy %	Error %	Time Taken in sec.
Removal of F7+F3	0.937	0.07	0.938	0.937	0.937	0.87	0.986	0.987	93.7103	6.2897	208.47
Removal of											
F7+FC5	0.927	0.08	0.929	0.927	0.927	0.85	0.983	0.984	92.74	7.26	194.78
Removal of											
F7+O2	0.939	0.066	0.94	0.939	0.939	0.88	0.985	0.986	93.9445	6.0555	202.76
Removal of											
F3+O2	0.947	0.057	0.948	0.947	0.947	0.89	0.989	0.989	94.714	5.286	209.24
Removal of											
F7+FC5+O2	0.92	0.089	0.921	0.92	0.919	0.84	0.979	0.98	91.9706	8.0294	184.06

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